Convolutional networks - theory

Convolutional network



Convolutional layers





Every neuron is connected with a (typically small) *receptive field* of neurons in the lower layer.

Neuron is "standard": Computes a weighted sum of its inputs, applies an activation function.

Convolutional layers

input neurons

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input neurons

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first hidden layer

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first hidden layer

Neurons grouped into *feature maps* sharing weights.

Convolutional layers



Each feature map represents a property of the input that is supposed to be spatially invariant.

Typically, we consider several feature maps in a single layer.

Pooling layers

hidden neurons (output from feature map)



Neurons in the pooling layer compute simple functions of their receptive fields (the fields are typically disjoint):

- Max-pooling : maximum of inputs
- L2-pooling : square root of the sum of squres
- Average-pooling : mean

• • • •

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- convolutional layer L_m: Neurons organized into disjoint feature maps, all neurons of a given feature map share weights (but have different inputs)
- pooling layer: "Neurons" organized into pooling maps, all neurons
 - compute a simple aggregate function (such as max),
 - have disjoint inputs.

Pooling after convolution is applied to each feature map separately.

I.e. a single pooling map after each feature map.

Denote

- X a set of input neurons
- Y a set of output neurons
- Z a set of all neurons $(X, Y \subseteq Z)$
- individual neurons denoted by indices i, j etc.
 - ξ_j is the inner potential of the neuron j after the computation stops

▶ *y_j* is the output of the neuron *j* after the computation stops

(define $y_0 = 1$ is the value of the formal unit input)

▶ *w_{ji}* is the weight of the connection **from** *i* **to** *j*

(in particular, w_{j0} is the weight of the connection from the formal unit input, i.e. $w_{j0} = -b_j$ where b_j is the bias of the neuron *j*)

- *j*← is a set of all *i* such that *j* is adjacent from *i* (i.e. there is an arc to *j* from *i*)
- *j*→ is a set of all *i* such that *j* is adjacent to *i* (i.e. there is an arc **from** *j* to *i*)
- [*ji*] is a set of all connections (i.e. pairs of neurons) sharing the weight w_{ji}.

Convolutional networks – activity

neurons of dense and convolutional layers:

inner potential of neuron j:

$$\xi_j = \sum_{i \in j_{\leftarrow}} w_{ji} y_i$$

• activation function σ_j for neuron *j* (arbitrary differentiable):

 $\mathbf{y}_j = \sigma_j(\xi_j)$

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Neurons of pooling layers: Apply the "pooling" function:

max-pooling:

$$y_j = \max_{i \in j_{\leftarrow}} y_i$$

avg-pooling:

$$y_j = \frac{\sum_{i \in j_{\leftarrow}} y_i}{|j_{\leftarrow}|}$$

A convolutional network is evaluated layer-wise (as MLP), for each $j \in Y$ we have that $y_j(\vec{w}, \vec{x})$ is the value of the output neuron j after evaluating the network with weights \vec{w} and input \vec{x} .

Convolutional networks – learning

Learning:

• Given a training set ${\mathcal T}$ of the form

$$\left\{ \left(\vec{x}_k, \vec{d}_k \right) \mid k = 1, \dots, p \right\}$$

Here, every $\vec{x}_k \in \mathbb{R}^{|X|}$ is an *input vector* end every $\vec{d}_k \in \mathbb{R}^{|Y|}$ is the desired network output. For every $j \in Y$, denote by d_{kj} the desired output of the neuron j for a given network input \vec{x}_k (the vector \vec{d}_k can be written as $(d_{kj})_{i \in Y}$).

Error function – mean squared error (for example):

$$E(\vec{w}) = \frac{1}{p} \sum_{k=1}^{p} E_k(\vec{w})$$

where

$$E_k(\vec{w}) = rac{1}{2} \sum_{j \in Y} \left(y_j(\vec{w}, \vec{x}_k) - d_{kj}
ight)^2$$

Convolutional networks – SGD

The algorithm computes a sequence of weight vectors $\vec{w}^{(0)}, \vec{w}^{(1)}, \vec{w}^{(2)}, \dots$

- weights in $\vec{w}^{(0)}$ are randomly initialized to values close to 0
- ▶ in the step t + 1 (here t = 0, 1, 2...), weights $\vec{w}^{(t+1)}$ are computed as follows:
 - Choose (randomly) a set of training examples $T \subseteq \{1, ..., p\}$
 - Compute

$$\vec{w}^{(t+1)} = \vec{w}^{(t)} + \Delta \vec{w}^{(t)}$$

where

$$\Delta \vec{w}^{(t)} = -\varepsilon(t) \cdot \frac{1}{|T|} \sum_{k \in T} \nabla E_k(\vec{w}^{(t)})$$

Here T is a *minibatch* (of a fixed size),

• $0 < \varepsilon(t) \le 1$ is a *learning rate* in step t + 1

► $\nabla E_k(\vec{w}^{(t)})$ is the gradient of the error of the example *k* Note that the random choice of the minibatch is typically implemented by randomly shuffling all data and then choosing minibatches sequentially. **Epoch** consists of one round through all data.

Recall that $\nabla E_k(\vec{w}^{(t)})$ is a vector of all partial derivatives of the form $\frac{\partial E_k}{\partial w_{ii}}$.

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First, switch from derivatives w.r.t. w_{ji} to derivatives w.r.t. y_j :

Recall that for every w_{ji} where j is in a dense layer, i.e. does not share weights:

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▶ Now for every *w_{ji}* where *j* is in a convolutional layer:

$$\frac{\partial E_k}{\partial \mathbf{w}_{ji}} = \sum_{r\ell \in [ji]} \frac{\partial E_k}{\partial \mathbf{y}_r} \cdot \sigma'_r(\xi_r) \cdot \mathbf{y}_\ell$$

Neurons of pooling layers do not have weights.

Now compute derivatives w.r.t. y_j:

for every
$$j \in Y$$
:
 $\frac{\partial E_k}{\partial y_j} = y_j - d_{kj}$

This holds for the squared error, for other error functions the derivative w.r.t. outputs will be different.

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for every j ∈ Z \ Y such that j[→] is either a dense layer, or a convolutional layer:

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for every j ∈ Z \ Y such that j[→] is max-pooling: Then j[→] = {i} for a single "max" neuron and we have

$$\frac{\partial E_k}{\partial y_j} = \begin{cases} \frac{\partial E_k}{\partial y_i} & \text{if } j = arg \ max_{r \in i_{\leftarrow}} y_r \\ 0 & \text{otherwise} \end{cases}$$

I.e. gradient can be propagated from the output layer downwards as in MLP.

- Conv. nets. are nowadays the most used networks in image processing (and also in other areas where input has some local, "spatially" invariant properties)
- Typically trained using backpropagation.
- Due to the weight sharing allow (very) deep architectures.
- Typically extended with more adjustments and tricks in their topologies.

The problem of cancer detection in WSI



The problem: Detect cancer in this image.

The problem of cancer detection in WSI



WSI annotated by pathologists, not pixel level precise!

Input data

WSI too large, 105,185 px x 221,772 px

Cut into patches of size 512 px x 512 px



Patch positive iff the inner square intersects the annotation

Training on WSI

Our dataset from Masaryk Memorial Cancer Insitute:

- 785 WSI from 166 patients
 (698 WSI for training, 87 WSI for testing)
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- Training data three step sampling:
 - 1. randomly select a label
 - 2. randomly select a slide containing at least a single patch with the label
 - 3. randomly select a patch with the label from the slide

VGG16



 3×3 convolutions, stride 1, padding 1. Max pooling $2\times 2,$ stride 2.

VGG16 pretrained on the ImageNet (of-the-shelf solution). Top fully connected parts removed, substituted with global max-pooling and a single dense layer.

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- The network has single logistic output the probability of cancer in the patch
- The error E = cross-entropy
- Training:
 - RMSprop optimizer
 - The "forgetting" hyperparameter: $\rho = 0.9$
 - ▶ The initial learning rate 5 × 10⁻⁵
 - If no improvement in E on validation data for 3 consecutive epochs ⇒ half the learning rate
 - If no improvement in ROCAUC on validation data for 5 consecutive epochs ⇒ terminate
 - Momentum with the weight $\alpha = 0.9$

Prediction



Model evaluation - attempt 1

Can we detect cancer somewhere in WSI?



Denote by *F* the function computed by our model. I.e., given a patch *I*, F(I) is the output value of the single output neuron with logistic activation function.
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Predict WSI positive iff at least one patch *I* satisfies $F(I) \ge t$ for a fixed threshold $t \in [0, 1]$.

Choosing t close to 1, we have achieved 100% accuracy, i.e., slide positive iff predicted positive. Problem solved ... No?

Can we detect cancer in patches?



Predict *I* positive iff $F(I) \ge 0.75$

Single WSI:







Ok, does it detect cancer?

Model evaluation – attempt 3 – FROC

Detect particular tumors ?



How to evaluate the quality of tumor detection?

Model evaluation – attempt 3 – FROC



sensitivity \approx the proportion of tumors containing at least one patch *I* with $F(I) \ge t$ w.r.t. all tumors in all slides

AvgFP \approx average number of patches *I* with $F(I) \ge t$ in each non-cancerous slide

Explainable methods (XAI)

The goal is to understand how and why the network does what it does.

We will consider classification models only.

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Methods based on various principles:

- Visualize weights and feature maps
- Visualize most important inputs for a given class
- Visualize the effect of input perturbations on the output
- Construct an intepretable surrogate model

Alex-net - filters of the first convolutional layer



- 64 filters of depth 3 (RGB)
- Combined each filter RGB channels into one RGB image of size 11x11x3.

CNN - feature maps





CNN - feature maps - radar target classification





Synthetic-aperture radar (SAR) – used to create two-dimensional images or three-dimensional reconstructions of objects, such as landscapes.

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- Denote by y_i(x) the value of the *output* neuron i ∈ Y on an input vector x.
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$$y_i(\vec{x}) - \lambda \left\| \vec{x} \right\|_2^2$$

over all input vectors \vec{x} .

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over all input vectors \vec{x} .

- A maximizing input vector computed using the gradient descent.
- Gives the most "representative" input vector of the class represented by the neuron *i*.

Maximizing input - example



dumbbell

cup

dalmatian

The goal: Label features in a given input that are "most important" for the output of the network.

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Various approaches:

- gradient based
 - Gradient saliency maps
 - GradCAM

▶ ...

- occlusion based
 - Simple occlusion maps
 - LIME
 - ▶ ...

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to measure the importance of the input y_k for the output y_i with respect to the particular input vector \vec{x} .

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Note that saliency comes from a surrogate local linear model given by the first-order Taylor approximation:

$$y_i(\vec{x}') \approx y_i(\vec{x}) + \left(\frac{\partial y_i}{\partial X}(\vec{x})\right)(\vec{x}' - \vec{x})$$

Here $\frac{\partial y_i}{\partial X}$ is the vector of all partial derivatives $\frac{\partial y_i}{\partial y_k}$ where $k \in X$.

Saliency maps - example







Saliency maps - example



Quite noisy, the signal is spread and does not say much about the perception of the owl.

Saliency maps - example



SmoothGrad:

- Do the following several times:
 - Add noise to the input image
 - Compute a saliency map
- Average the resulting saliency maps.

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ALL values of all neurons y_j are computed on the input *I*.

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Fix a convolutional layer L consisting of convolutional feature maps F¹,..., F^k.

Each F^{ℓ} is a set of neurons that belong to the feature map F^{ℓ} . Slightly abusing notation, we write $F^{\ell}(I)$ to denote the tensor of all values of all neurons in $F^{\ell}(I)$.

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- Fix an output neuron $i \in Y$ with the value y_i .
- Compute the average importance of $F^{\ell}(I)$ for the output y_i :

$$\alpha_i^\ell = \frac{1}{|F^\ell|} \sum_{j \in F^\ell} \frac{\partial y_i}{\partial y_j}(I)$$

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and the final gradCAM heat map for L is obtained using

$$M_i^L = \operatorname{ReLU}\left(\sum_{\ell=1}^k \alpha_i^\ell F^\ell(I)\right)$$

GradCAM on VGG16



GradCAM on VGG16



Consider the last convolutional layer of the VGG16 (Block5, Conv3)

GradCAM on VGG16



From left to right:

- An image of a cat (has to be resized to 224 × 224 to fit VGG16)
- The gradCAM heat map for the last convolutional layer and the class "cat"
- Rescaled and smoothed gradCAM heat map.
- The gradCAM overlay.

- Systematically cover parts of the input image.
- Observe the effect on the output value.
- Find regions with the largest effect.

Occlusion - example


['harmonica, mouth organ, harp, mouth harp']





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Outline:

- Consider superpixels of I as interpretable components.
- Construct a linear model approximating the network aroung the image *I* with weights corresponding to the superpixels.
- Select the superpixels with weights of large magnitude as the important ones.



Original Image



Interpretable Components

Superpixels as interpretable components



Original Image



Interpretable Components

Denote by P_1, \ldots, P_ℓ all superpixels of *I*.

Superpixels as interpretable components



Original Image



Interpretable Components

Denote by P_1, \ldots, P_ℓ all superpixels of *I*. Consider binary vectors $\vec{x} = (x_1, \ldots, x_\ell) \in \{0, 1\}^\ell$.

Superpixels as interpretable components



Original Image



Interpretable Components

Denote by P_1, \ldots, P_ℓ all superpixels of *I*.

Consider binary vectors $\vec{x} = (x_1, \dots, x_\ell) \in \{0, 1\}^\ell$.

Each such vector \vec{x} determines a "subimage" $I[\vec{x}]$ of I obtained by removing all P_k with $x_k = 0$.





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LIME

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- Given the image I to be interpreted, consider the following training set:

$$\mathcal{T} = \left\{ (\vec{x}_1, y_i(I[\vec{x}_1])), \dots, (\vec{x}_p, y_i(I[\vec{x}_p])) \right\}$$

Here $\vec{x}_h = (x_{h1}, \dots, x_{h\ell})$ are (some) binary vectors of {0, 1}. E.g., randomly selected.



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- Train a linear model (ADALINE) with weights w₀, w₁,..., w_l on T minimizing the mean-squared error (+ a regularization term making the number of non-zero weights as small as possible).
 Intuitively, the linear model approximates the networks on "subimages" of *I* obtained by removing "unimportant" superpixels.
- Inspect the weights (magnitude and sign).





Original Image P(tree frog) = 0.54





Explanation



(a) Original Image

(b) Explaining Electric guitar (c) Explaining Acoustic guitar

(d) Explaining Labrador



(a) Husky classified as wolf

